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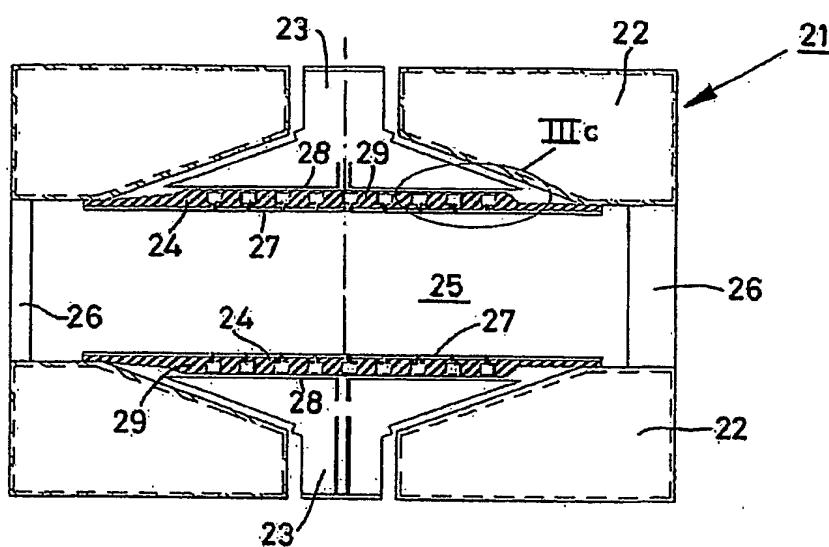
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(54) Title: MAGNETIC RESONANCE IMAGING DEVICE WITH SOUND-ABSORBING MEANS



(57) Abstract: The invention provides a magnetic resonance imaging (MRI) device (21), comprising a diagnostic space (25), a main magnetic system (22) for generating a main magnetic field in said diagnostic space, a gradient magnetic coil system (23) comprising a gradient coil for generating at least one gradient of the main magnetic field, and noise reducing means (29, 32) for reducing noise that is generated as a result of vibrations of the gradient coil. The noise reducing means comprise a sound-absorbing panel (29) disposed between the gradient coil and the diagnostic space. The sound-absorbing panel (29) comprises channels having an open end and a closed end.



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MAGNETIC RESONANCE IMAGING DEVICE WITH SOUND-ABSORBING MEANS

The invention relates to a magnetic resonance imaging (MRI) device, comprising a diagnostic space, a main magnetic system for generating a main magnetic field in said diagnostic space, a gradient magnetic coil system comprising a gradient coil for generating at least one gradient of the main magnetic field, and noise reducing means for 5 reducing noise that is generated as a result of vibrations of the gradient coil.

A magnetic resonance imaging (MRI) device of the kind mentioned in the opening paragraph is known in a substantially cylindrical embodiment thereof, which is also 10 referred to as the closed type. An example thereof is disclosed in US Pat. No. 6,043,653. In the case of closed-type MRI devices, an asymmetrical arrangement may be used, seen in the direction of rotation, in which the device has a strongly flattened underside or an oval cross-section, for example.

Besides that, we have lately witnessed a growing interest in the open variant, 15 which comprises two substantially disc-shaped housings, each accommodating part of the main magnetic system and part of the gradient magnetic system. The diagnostic space is positioned between the disc-shaped housings, where a vertically oriented magnetic field is generated. An open-type MRI system has a few significant advantages over the closed-type MRI system, which advantages are connected with the fact that more free space is available 20 round the patient in the diagnostic space. On the one hand this helps to alleviate any claustrophobic feelings that the patient may have, whilst on the other hand the larger amount of space makes it possible or easier for medical staff to perform medical actions on the patient in the diagnostic space.

An important problem that is encountered in practice are the acoustic 25 vibrations produced by the MRI system. Said acoustic vibrations produce noise, which is unpleasant for the patient who is to be examined in the diagnostic space. The acoustic vibrations are caused by the fact that relatively high Lorentz forces act on the electrical windings of the gradient coil as a result of electro-mechanical interaction between the alternating current being passed through the electrical windings of the gradient coil at

5 frequencies of up to about 4000 Hz and the strong magnetic field generated by the main magnet. Said interaction causes mechanical vibrations in the construction of the MRI system, more specifically in the gradient coil thereof, which in turn lead to the occurrence of said acoustic vibrations both in the diagnostic space and outside the MRI system, precisely in the frequency range of up to 4000 Hz in which a person's sense of hearing is acutest.

The aforesaid US Pat. No. 6,043,653 proposes a solution for the noise problem, according to which the gradient coil windings as a whole are accommodated in a vacuum chamber. This makes heavy constructional demands on the MRI device in question, which leads to a significant increase in the cost price thereof.

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An object of the invention is to provide a magnetic resonance imaging (MRI) device of the kind mentioned in the opening paragraph with a reduced noise level in a relatively simple and thus relatively inexpensive manner.

15 In order to achieve this object, a magnetic resonance imaging (MRI) device according to the invention is characterized in that the noise reducing means comprise a sound-absorbing panel disposed between the gradient coil and the diagnostic space. Thus, a substantial noise reduction can be achieved in a constructionally simple manner which, unlike the solution proposed in the aforesaid US Pat. No. 6,043,653, which attempts to 20 prevent sound being produced, prevents sound from being reflected by absorbing said sound by means of the sound-absorbing panel that its disposed precisely at the location where its effect will be greatest.

25 A noticeable noise reduction is already obtained if the sound-absorbing panel has an absorption coefficient in the order of at least 0.5, more preferably in the order of at least 0.75 for at least part of the frequency range between 20 Hz and 4000 Hz. The sound absorption coefficient indicates the proportion between absorbed sound (in dB) and incoming sound (in dB). If the absorption coefficient is 1, this implies, therefore, that the sound-absorbing panel absorbs all the incoming sound. A sound absorption coefficient value of 0.5 will result in a noise reduction of 1.3 dB. In general, the following applies as regards the 30 sound pressure SPL (in Pa) as a function of the time t:

$$SPL(t) = A * [\sin(2\pi*f*t) + \sqrt{(1-\alpha)*\sin^2(2\pi*f*t)}]$$

wherein A is the amplitude of a sound wave (in Pa), f is the frequency, and α is the absorption coefficient.

A very suitable embodiment of a magnetic resonance imaging device according to the invention is obtained if the sound-absorbing panel comprises channels 5 having an open end and a closed end, which channels preferably extend at least substantially in a direction parallel to the direction between the diagnostic space and the gradient coil. The channels' function is to effect a certain degree of sound absorption by the panels. An important advantage of the use of channels is that a suitable selection of the dimensions of said channels makes it possible to optimize the sound-absorbing effect for the specific 10 eigenfrequency of the gradient coil in the audible range.

Dependent on the available space for the required channels and the required length thereof, it might be advantageous if the channels extend at least substantially perpendicularly to the direction between the diagnostic space and the gradient coil, at least on the side of their closed ends.

15 The open ends of at least some of the channels are preferably present on the side of the associated channels that faces the diagnostic space. Thus, sound coming from the diagnostic space will be absorbed.

Alternatively, but in particular in combination with the preferred embodiment as mentioned above, it is also quite possible within the framework of the invention for the 20 open ends of at least some of the channels to be present on the side of the associated channels that faces towards the gradient coil. Thus, the open ends are directed towards the source of the noise, so that a very advantageous noise reducing effect is obtained. If channels having their open ends on the side facing towards the diagnostic space as well as channels having their open ends on the side facing towards the gradient coil are used, it is possible, of course, 25 to adapt the proportion between such channels to the production of noise associated with a specific MRI device.

As already said before, a suitable dimensioning of the channels makes it possible to optimally adapt the sound-absorbing effect thereof to the eigenfrequencies that occur. In general it can be stated, however, that the degree of sound absorption increases as 30 the cross dimensions of the channels on the side of the associated open ends decrease. Consequently, the cross dimension of at least a part of the channels on the side of the associated open ends is preferably maximally 15 mm, more preferably maximally 10 mm. In the case of a channel in the form of a cylindrical bore, the term cross dimension refers to the diameter, of course. Although it is not necessary within the framework of the invention for

the channels to be substantially cylindrical, a cylindrical shape is the most advantageous shape from a manufacturing viewpoint.

According to a very advantageous preferred embodiment, a cross dimension of a part of the channels on the side of the associated closed ends thereof is different from a cross dimension of the part of the channels on the side of the associated open ends. Thus, relatively short lengths of the associated channels provide a relatively great sound-absorbing effect. This is a major advantage in particular in the case of MRI equipment, since space is usually not available, or it can only be made available at major cost.

Preferably, the cross dimension of the part of the channels on the side of the associated closed ends is larger than a cross dimension of the part of the channels present on the side of the associated open ends. Channels configured in this manner, in which sound travels from a relatively small passage to a wider space at the end of the channel, appear to be very effective in absorbing sound without a great length of the channels being required.

In order to achieve a maximum utilization of the sound-absorbing effect, the proportion between the cross dimension of the part of the channels on the side of the associated closed ends and the cross dimension of the part of the channels on the side of the associated open ends is preferably in the order of 2.5, more preferably at least in the order of 4.0.

The sound-absorbing effect can be further enhanced by realizing a high density of sound-absorbing channels. Within this framework, the minimum spacing between adjacent channels at the location of the associated maximum cross dimension of the adjacent channels is preferably maximally 50% of the sum of the associated maximum cross dimensions, more preferably maximally 35% of the sum of the associated maximum cross dimensions. This implies, for example, that the spacing between two adjacent channels having a maximum diameter of 100 mm and 60 mm, respectively, is preferably maximally 80 mm, more preferably maximally 56 mm.

The above example perfectly illustrates that it is not necessary within the framework of the invention for the channels of the sound-absorbing panel to have mutually corresponding dimensions. On the contrary, it will generally be advantageous to use mutually different dimensions for the channels, since this makes it possible to optimally adapt the sound-absorbing effect of the channels to the various eigenfrequencies in the audible range of the gradient coil. Consequently, a very advantageous embodiment of the invention is characterized in that the dimensions of the channels of the sound-absorbing panel are mutually different.

In order to limit the additional amount of space taken up as a result of the use of the sound-absorbing panel comprising the channels as much as possible, or even prevent this altogether, it is furthermore quite preferable to provide the sound-absorbing panel with a radio frequency transmission coil system for generating and/or receiving a radio frequency signal in the diagnostic space. The function and the necessity of a radio frequency transmission coil system in an MRI device is known to those skilled in the art, and thus requires no further explanation herein. It suffices to say that the radio frequency transmission coil system is usually present between the gradient coil and the diagnostic space. The exact embodiment of the radio frequency transmission coil system is not of primary interest within the framework of the present preferred embodiment of the invention. The radio frequency coil of the radio frequency transmission coil system may be symmetrical or asymmetrical, for example, it may or may not be provided with shoulder recesses, or it may only be present on one side of the MRI device, for example.

Preferably, the radio frequency transmission coil system comprises an electrically conductive winding which extends at least in part between at least some of the channels. Furthermore preferably, such an electrically conductive winding extends in full between at least some of the channels. In practice, this preferred embodiment will be used in particular with closed-type MRI devices, in which the radio frequency transmission coil system comprises electrically conductive windings.

In the case of open-type MRI devices, the radio frequency transmission coil system in general comprises an electrically conductive layer arranged on a plate-shaped carrier of a resinous material. Such a carrier can be advantageously provided with sound-absorbing channels, so that the carrier can be regarded as the sound-absorbing panel within the framework of the present invention. Preferably, the radio frequency transmission coil system therefore comprises at least one electrically conductive layer, with which the sound-absorbing panel is coated on the side of the diagnostic space and in which openings are present at the location of any open ends of the channels that may be present on the side of the diagnostic space. Said openings in the electrically conductive layer guarantee the open character of one end of the channels. The open ends of the channels being used may all be present on the side of the gradient coil, of course, in which situation it is therefore not necessary to provide the electrically conductive layer with openings.

In particular if it is decided to have the cross dimensions of the channels change in leaps, seen in the longitudinal direction thereof, it is preferable for manufacturing

reasons to build up the sound-absorbing panel of a number of abutting, preferably glued-together subpanels.

A further improvement as regards the sound absorbing or noise reducing effect is obtained if, in accordance with a preferred embodiment, the sound-absorbing panel is 5 coated between the open ends with a sound-absorbing material having an absorption coefficient of at least 0.5 for at least part of the frequency range between 20 Hz and 4000 Hz.

In an alternative embodiment of the sound-absorbing panel, said panel comprises glass wool. The use of glass wool is in particular advantageous in the frequency range between 2000 Hz and 10.000 Hz.

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The invention will be explained in more detail hereinafter by means of a description of a number of preferred embodiments of the invention. In the description, reference will be made to the following Figs., in which:

15 Fig. 1 is a schematic, vertical cross-sectional view of a first embodiment of a (closed-type) MRI device according to the invention;

Fig. 2 is a schematic, vertical cross-sectional view of a second embodiment of a (closed-type) MRI device according to the invention;

20 Fig. 3a is a schematic, vertical cross-sectional view of a third embodiment of a (closed-type) MRI device according to the invention;

Fig. 3b is a front elevation of a radio frequency transmission coil unit as used in the MRI device according to Fig. 3a;

Fig. 3c shows the detail IIIc in Fig. 3a; and

25 Figs. 4a-4c shows three alternative embodiments of sound-absorbing channels that may be used in preferred embodiments of the present invention.

Figure 1 schematically shows in a vertical cross-sectional view the structure of an MRI device 1 according to the invention. A cylindrical, main magnetic system 2 is shown 30 to form the outermost shell. Said cylindrical main magnetic system 2 comprises superconducting magnets, which are maintained at a low temperature, using a cryostat, such that said magnets will exhibit their superconducting characteristics. Present within the main magnetic system 2 is a cylindrical gradient coil system 3. A cylindrical radio frequency transmission coil system 4, a few details of which are schematically shown in figure 1, is in

turn present within the gradient coil system 3. Finally, the diagnostic space 5, in which the patient lies on a support (not shown), is present within the substantially cylindrical radio frequency transmission coil system. Such a structure of a closed-type MRI device is known to those skilled in the art. An illustrative example of this is the aforesaid US Pat. No. 5 6,043,653, for example. Consequently, a brief explanation of the structure of the MRI device 1 will suffice within the framework of the present invention.

The main magnetic system 2 generates a main magnetic field in the diagnostic space 5. Within the framework of the present invention it suffices to mention that it is possible, using the main magnetic system 2, the gradient coil system 3 and the radio frequency transmission coil system 4, to generate images of internal parts of a patient who is present in the diagnostic space 5. Said generation of images may involve very large electromagnetic forces, which cause vibrations of the gradient coil system 3. Said vibrations have a frequency within the audible range of humans, in particular in the frequency range between 20 Hz and 4000 Hz, and they constitute a substantial, unpleasant acoustic burden, at least in principle, for a patient who is present in the diagnostic space 5.

The cylindrical radio frequency transmission coil system 4 is substantially made up of a tubular shell of a solid resinous material 6. Embedded in said resinous material are electrically conductive windings 7. The windings 7 extend substantially in the axial direction. Present between the windings 7 are radially extending cylindrical bores 8, which are open at the ends facing the cylindrical gradient coil system 3 and which are closed at the opposite ends. The length of the bores 8 is less than the thickness of the wall of resinous material 6 of the radio frequency transmission coil system 4. The bore has a relatively small diameter in the order of 20 mm on the side of the open end, whereas the diameter on the side of the closed end is about 100 mm. An abrupt diameter leap occurs between the two parts of the bores 8 that have different diameters.

It has been established by experiment that bores 8 have an absorbing effect on sound from the gradient coil system 3. The dimensions of the bores 8 determine for which frequencies the sound-absorbing effect occurs in particular, so that the sound-absorbing effect can be optimized for the eigenfrequencies of the gradient coil system 3, insofar as they fall within the audible range, by suitably selecting the dimensions of the bores 8 (the diameters and the individual lengths of parts having a particular diameter).

Figure 2 shows a cross-sectional view similar to figure 1, with this difference that figure 2 shows a MRI device 11 whose only difference from the MRI device 1 relates to the embodiment of the radio frequency transmission coil system 14. More specifically, the

two embodiments differ from each other as regards the orientation of the bores 18 of the radio frequency transmission coil system 14, whose open ends are not exclusively present on the side of the cylindrical gradient coil system 3, but alternately on the side of the cylindrical coil system 3 and on the side of the diagnostic space 5. The bores 18 have identical 5 dimensions, although this is not necessary within the framework of the invention. Since the open ends are present on either side (seen in radial direction) of the radio frequency transmission coil system 14, the sound-absorbing effect occurs for sound coming from the direction of the cylindrical gradient coil system 3 as well as for sound coming from the direction of the diagnostic space 5.

10 Figure 3a schematically shows in a cross-sectional view a MRI device 21 according to the invention. The MRI device 21 is of the open type. Although it is of different design than a close-type MRI device, the open-type MRI device 21 comprises the same main components as a closed-type MRI device, viz. a main magnetic system 22, a gradient coil system 23 and a radio frequency transmission coil system 24. The systems 22, 23, 24 are 15 mainly made in two parts disposed on either side of a diagnostic space 25. The parts of the systems 22, 23, 24 present at the bottom side of the diagnostic space 25 are accommodated in a substantially disc-shaped lower housing (not shown), whilst the parts of the systems 22, 23, 24 present at the upper side of the diagnostic space are accommodated in a substantially disc-shaped upper housing (not shown). The lower housing and the upper housing are 20 interconnected by means of uprights 26. A more detailed description of an open-type MRI device is not necessary herein, in the first place because open-type MRI devices are generally known to those skilled in the art and in the second place because no further explanation is required for understanding the invention.

25 The radio frequency transmission coil system 24 comprises two substantially disc-shaped, more or less solid plates 29 of a resinous material, which are disposed on either side of the diagnostic space 25. Within the framework of the invention it is not important for the preferred embodiment, in which sound absorbing bores are formed in the radio frequency transmission coil system, whether said plates are solid or made of a resinous material.

30 Alternatively it is possible, for example, to use polycarbonate, which does not necessarily have to be solid. The windings 7 as used in the MRI devices 1 and 11 according to figures 1 and 2, respectively, have been substituted for electrically conductive plates 27 on the side of the diagnostic space 25. An electrically conductive plate 28 is also present on the side of system parts of the radio frequency transmission coil system 24 remote from the diagnostic

space 25, which electrically conductive plate is significantly less thick than the electrically conductive plates 27, however.

Present between the two electrically conductive plates 27, 28 is a carrier plate 29 of a resinous material, which is built up of two glued-together subplates 30, 31. Bores 32 having an open end on the side of the diagnostic space 25 and an opposite closed end are formed in the carrier plates 29. The diameter of the bore 32 extending within the thickness of the subplate 31 is smaller than the diameter of the bore 32 extending within the thickness of the subplate 30. Consequently, a diameter leap occurs within the length of the bore 32 at the location of the transition between the subplates 30 and 31, which is advantageous for understandable manufacturing reasons. At the location of the open ends of the bores 32, the electrically conductive plate 27 is likewise provided with openings having a diameter corresponding to that of the bore 32 extending within the subplate 31.

As already said forth above, the presence of the bores 32 provides a sound-absorbing effect, in this case for sound coming from the diagnostic space 25. Alternatively, as a person skilled in the art will understand, the open ends of the bores 32 may be directed towards an associated part of the gradient coil system 23, or alternately towards the associated part of the gradient coil system 23 and towards the diagnostic space 25, more or less similar to the situation of the MRI device 11 according to figure 2.

Figure 3b is a clear schematic view of the manner in which the bores are distributed over the area of the system parts of the radio frequency coil system 24. Although this is not essential to the invention, it has been opted to use a constant centre-to centre distance between the various bores 30. In explanation thereof it is noted that the large diameters (not shown) on the side of the closed ends of the bores 30 are illustrated in dotted lines in figure 3. As the figure shows, the bores 30 are different from each other as regards the dimension of the diameters at the location of the open ends and the closed ends. Thus, the bores and the sound-absorbing effects thereof can be optimally adapted to the various eigenfrequencies that occur in the gradient coil system 23. Besides the diameters of the various parts, also the length of said parts, can be varied.

Figures 4a-4c show alternative embodiments of sound-absorbing channels that may be used in a sound-absorbing panel that forms part of a MRI device according to the present invention. The channel 40 that is shown in figure 4a extends between an open end 41 and a closed end 42 within a sound-absorbing panel 43 having a free surface 44. The channel 40, which has a circular cross-section, comprises a right angle between the two ends 41 and 42, so that part of the necessary length of the channel 40, which is not available within the

sound-absorbing panel 43 in a direction perpendicular to the free surface 44, is created in a direction parallel to the free surface 44.

The sound-absorbing panel 50 having a free surface 51 as shown in figure 4b comprises a sound-absorbing channel 52 having one open end 53 and two closed ends 54, 55.

5 On the side of the open end 53, the channel 52 comprises a single cylindrical space 56, which branches into cylindrical spaces 57, 58 of mutually different diameter and length on the side of the closed ends 54 and 55, respectively. The sound absorbing channel 52 can be geared to the attenuation of specific frequencies by varying the dimensions of the spaces 56, 57, 58.

The diameter of the sound-absorbing channel 60 according to figure 4c increases in steps from the open end 61 to the closed end 62 thereof, so that three parts 63, 64, 65 having different diameters are formed.

Although the invention has been explained in the above on the basis of the use of bores for obtaining a sound-absorbing effect, it is also possible within the framework of the invention to use sound-absorbing materials, such as glass wool. Also a combination is 15 possible, in which the sound-absorbing material, such as glass wool, is provided around the open ends of the various bores.

CLAIMS:

1. A magnetic resonance imaging (MRI) device, comprising a diagnostic space, a main magnetic system for generating a main magnetic field in said diagnostic space, a gradient magnetic coil system comprising a gradient coil for generating at least one gradient of the main magnetic field, and noise reducing means for reducing noise that is generated as a result of vibrations of the gradient coil, characterized in that the noise reducing means comprise a sound-absorbing panel disposed between the gradient coil and the diagnostic space.
5
2. A magnetic resonance imaging (MRI) device according to claim 1, characterized in that the sound-absorbing panel has an absorption coefficient in the order of at least 0.5, more preferably in the order of at least 0.75 dB for at least part of the frequency range between 20 Hz and 4000 Hz.
10
3. A magnetic resonance imaging (MRI) device according to claim 1 or 2, characterized in that the sound-absorbing panel comprises channels having an open end and a closed end.
15
4. A magnetic resonance imaging (MRI) device according to claim 3, characterized in that said channels extend at least substantially in a direction parallel to the direction between the diagnostic space and the gradient coil.
20
5. A magnetic resonance imaging (MRI) device according to claim 3 or 4, characterized in that the channels extend at least substantially perpendicularly to the direction between the diagnostic space and the gradient coil, at least on the side of their closed ends.
25
6. A magnetic resonance imaging (MRI) device according to claim 3, 4 or 5, characterized in that the open ends of at least some of the channels are present on the side of the associated channels that faces towards the diagnostic space.

7. A magnetic resonance imaging (MRI) device according to claim 3, 4 or 5, characterized in that the open ends of at least some of the channels are present on the side of the associated channels that faces towards the gradient coil.

5 8. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 7, characterized in that the cross dimension of at least a part of the channels on the side of the associated open ends is maximally 15 mm, preferably maximally 10 mm.

10 9. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 8, characterized in that the cross dimension of at least a part of the channels on the side of the associated closed ends thereof is different from a cross dimension of the part of the channels on the side of the associated open ends.

15 10. A magnetic resonance imaging (MRI) device according to claim 9, characterized in that the cross dimension of the part of the channels on the side of the associated closed ends is larger than a cross dimension of the part of the channels present on the side of the associated open ends.

20 11. A magnetic resonance imaging (MRI) device according to claim 10, characterized in that the proportion between the cross dimension of the part of the channels on the side of the associated closed ends and the cross dimension of the part of the channels on the side of the associated open ends is at least in the order of 2.5, preferably at least in the order of 4.0.

25 12. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 9, characterized in that the minimum spacing between adjacent channels at the location of the associated maximum cross dimension of the adjacent channels is maximally 50% of the sum of the associated maximum cross dimensions, preferably maximally 35% of the sum of the associated maximum cross dimensions.

30 13. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 12, characterized in that the dimensions of the channels of the sound-absorbing panel are mutually different.

14. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 13, characterized in that the sound-absorbing panel is provided with a radio frequency transmission coil system for generating and/or receiving a radio frequency signal in the diagnostic space.

5

15. A magnetic resonance imaging (MRI) device according to claim 14, characterized in that the radio frequency transmission coil system comprises an electrically conductive winding which extends at least in part between at least some of the channels.

10 16. A magnetic resonance imaging (MRI) device according to claim 14, characterized in that the radio frequency transmission coil system comprises at least one electrically conductive layer, with which the sound-absorbing panel is coated on the side of the diagnostic space and in which openings are present at the location of any open ends of the channels that may be present on the side of the diagnostic space.

15

17. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 16, characterized in that the sound-absorbing panel is built up of a number of abutting, preferably glued-together subpanels.

20 18. A magnetic resonance imaging (MRI) device according to any one of the claims 3 - 17, characterized in that the sound-absorbing panel is coated between the open ends with a sound-absorbing material having an absorption coefficient of at least 0.5 for at least part of the frequency range between 20 Hz and 4000 Hz.

25 19. A magnetic resonance imaging (MRI) device according to any one of the preceding claims, characterized in that said sound-absorbing panel comprises glass wool.

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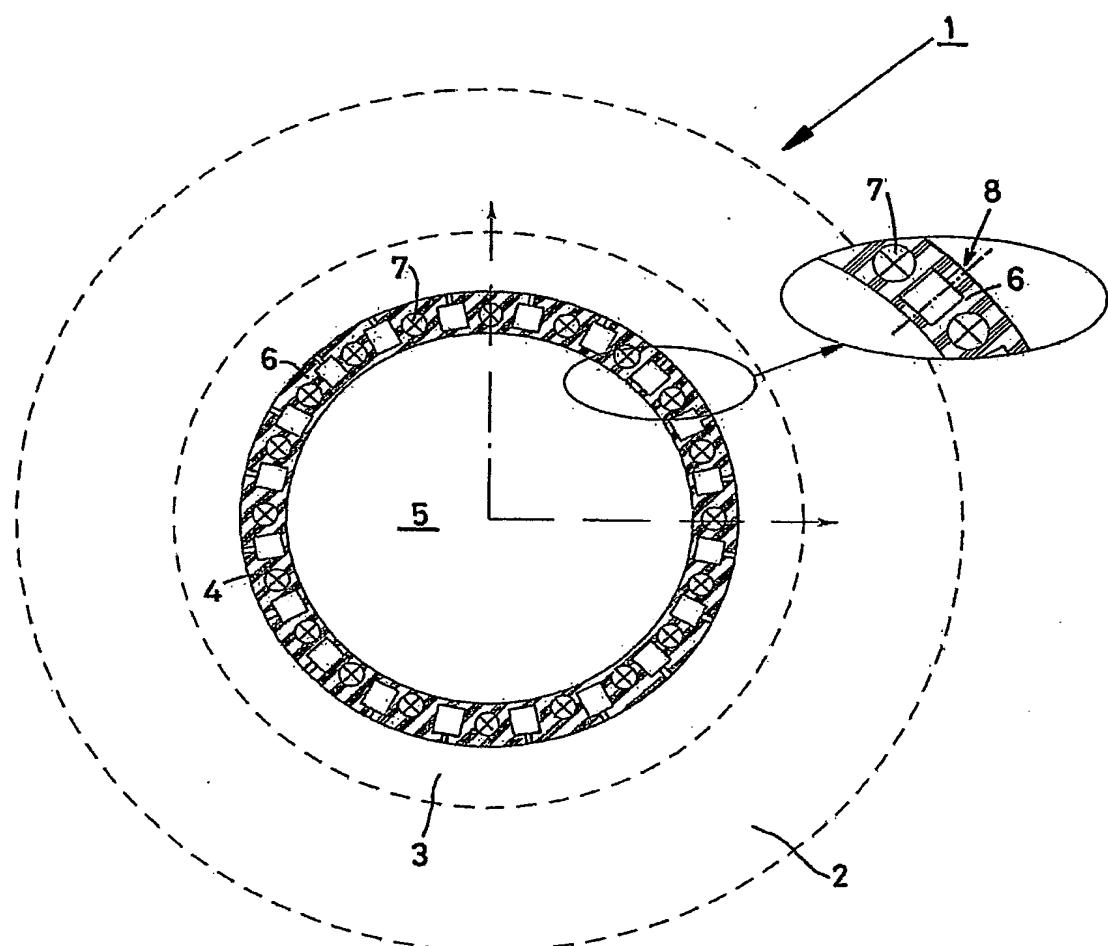


FIG.1

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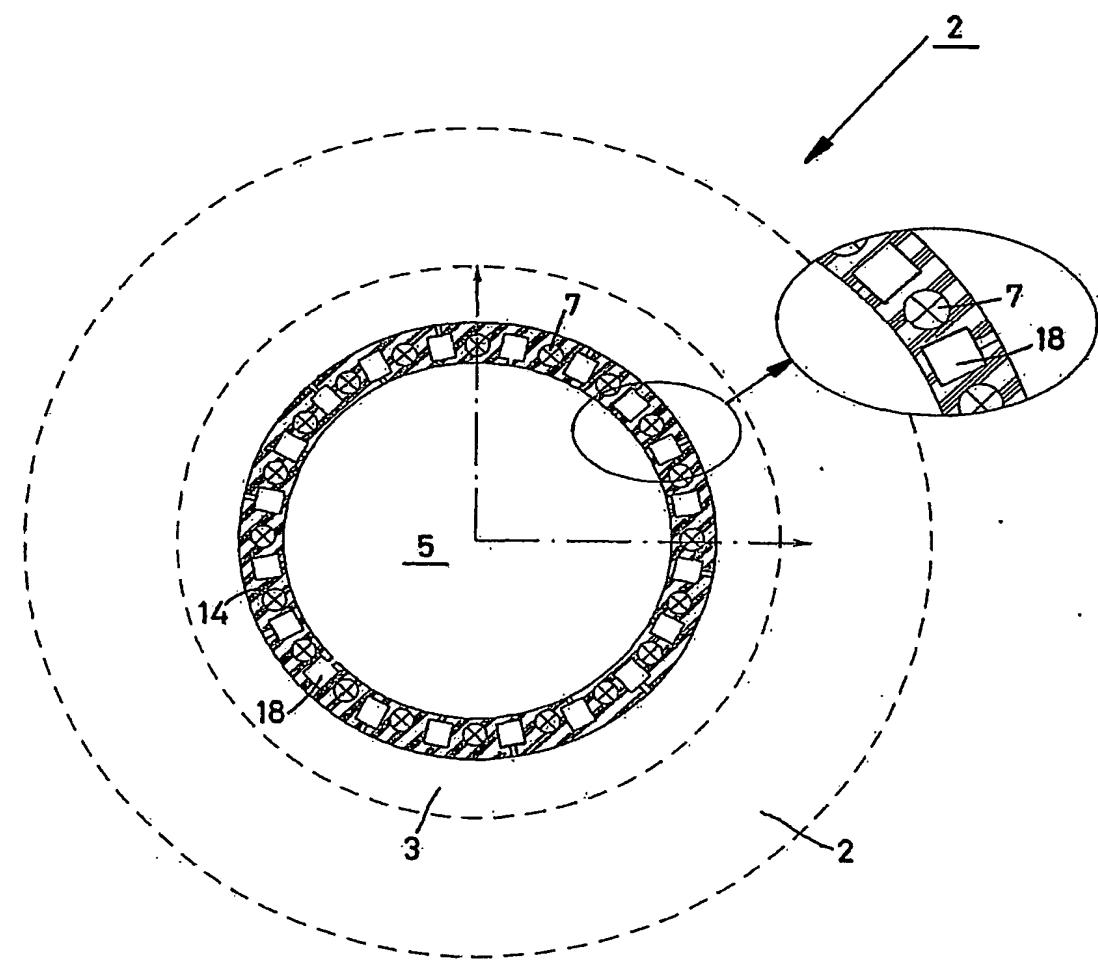
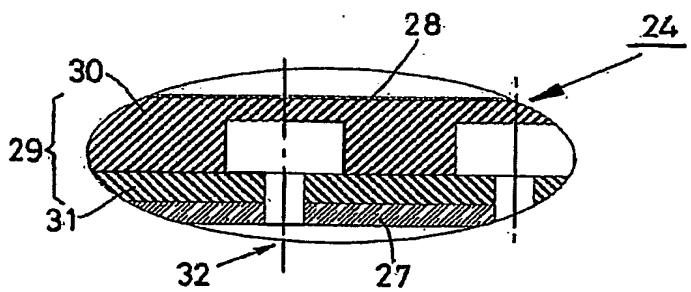
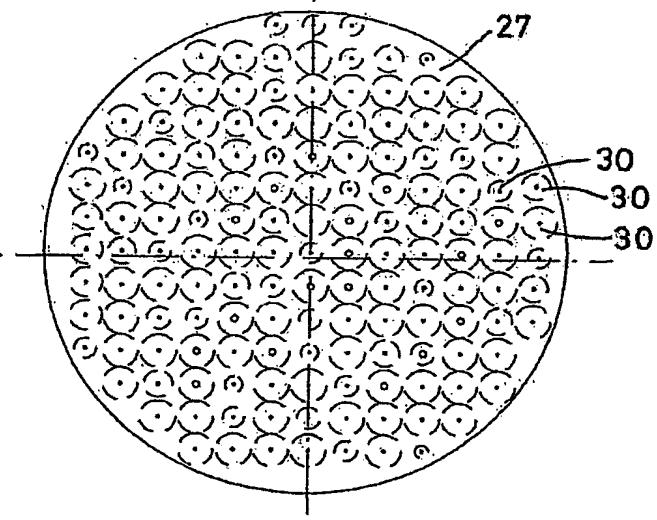
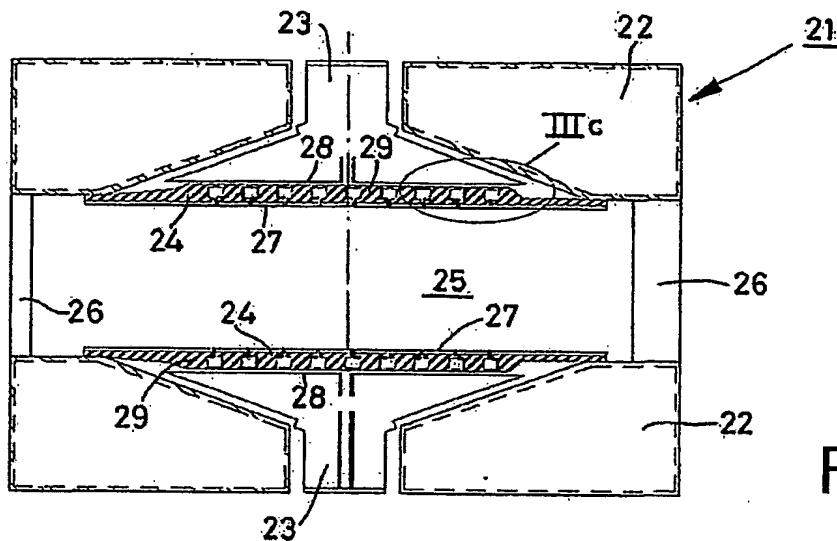


FIG.2

3/4



4/4

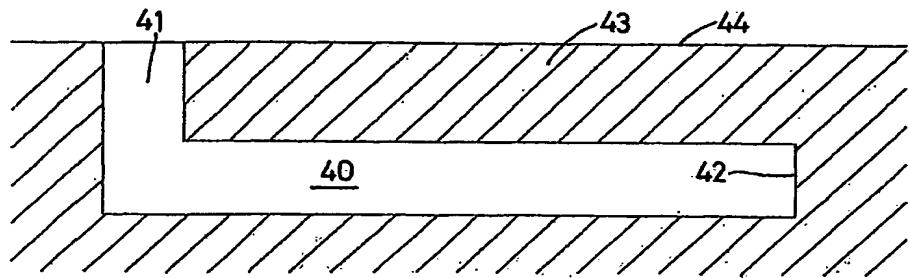


FIG. 4a

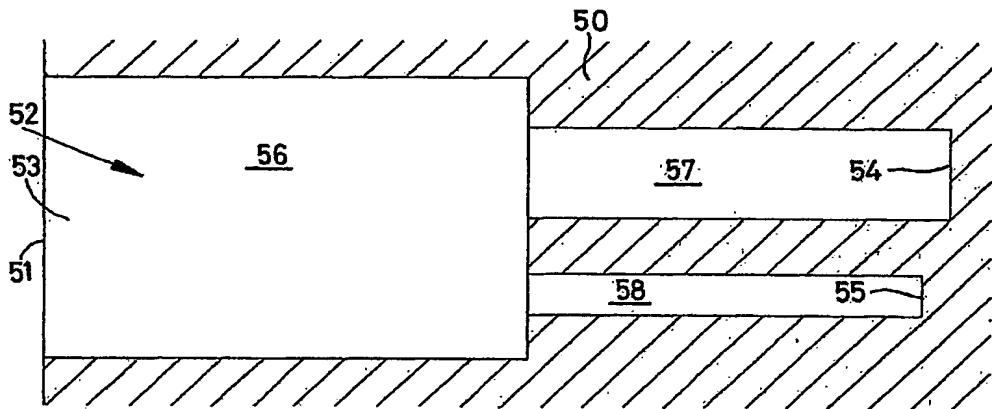


FIG. 4b

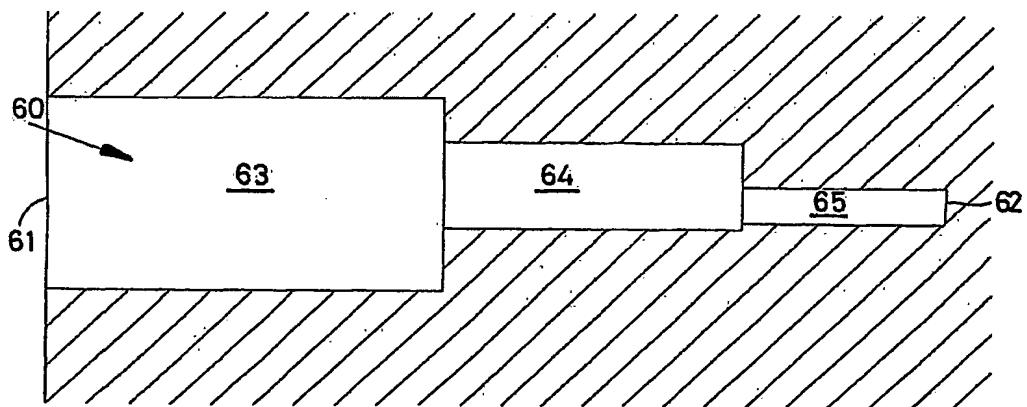


FIG. 4c

INTERNATIONAL SEARCH REPORT

International Application No
.../IB2004/050709A. CLASSIFICATION OF SUBJECT MATTER
IPC 7 G01R33/385

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 7 G01R

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the International search (name of data base and, where practical, search terms used)

EPO-Internal, PAJ, INSPEC, MEDLINE, EMBASE, BIOSIS, WPI Data, COMPENDEX

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 6 414 489 B1 (RADZIUN MICHAEL J ET AL) 2 July 2002 (2002-07-02)	1,2
Y	column 3, line 52 - column 4, line 6; figures 1,2 -----	3-12,14, 15,17
Y	US 2003/016018 A1 (ARZ WINFRIED) 23 January 2003 (2003-01-23) paragraph '0008! - paragraph '0013! paragraph '0022! -----	3-12,14, 15,17
X	DE 198 38 390 A (SIEMENS AG) 2 March 2000 (2000-03-02)	1,2
A	column 3, line 18 - line 20 column 3, line 49 - line 55 ----- -/-	3-19



Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

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Date of the actual completion of the international search	Date of mailing of the international search report
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Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo nl, Fax (+31-70) 340-3016	Authorized officer Skalla, J
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INTERNATIONAL SEARCH REPORT

International Application No
PCT/IB2004/050709

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 084 676 A (SAHO NORIHIDE ET AL) 28 January 1992 (1992-01-28) column 3, line 51 - line 66 column 6, line 57 - column 7, line 44	1,2,19
A	column 3, line 51 - line 66 column 6, line 57 - column 7, line 44	3-18
X	EP 0 350 640 A (TOKYO SHIBAURA ELECTRIC CO) 17 January 1990 (1990-01-17) page 5, line 8 - line 49	1,2
A	page 10, line 34 - line 37	3-19
X	PATENT ABSTRACTS OF JAPAN vol. 2002, no. 07, 3 July 2002 (2002-07-03) -& JP 2002 085368 A (GE MEDICAL SYSTEMS GLOBAL TECHNOLOGY CO LLC), 26 March 2002 (2002-03-26)	1,2
A	abstract	3-19
X	EP 0 522 742 A (HITACHI LTD) 13 January 1993 (1993-01-13) column 6, line 20 - line 44	1,2
A	column 6, line 20 - line 44	3-19
X	PATENT ABSTRACTS OF JAPAN vol. 012, no. 108 (E-597), 7 April 1988 (1988-04-07) -& JP 62 239503 A (HITACHI LTD), 20 October 1987 (1987-10-20)	1,2
A	abstract	3-19
X	DE 34 44 388 A (OXFORD MAGNET TECH) 1 August 1985 (1985-08-01)	1,2
A	page 10, last paragraph - page 11, last paragraph	3-19
X	US 4 774 486 A (MORITSU KAZUKI) 27 September 1988 (1988-09-27) column 2, line 61 - line 65	1,2
X	US 5 256 969 A (MIYAJIMA GOH ET AL) 26 October 1993 (1993-10-26)	1,2,19
A	column 2, line 20 - line 32	3-18
	column 3, line 43 - line 50	
	column 6, line 30 - line 66	
A	YODA M ET AL: "Tunable acoustic absorber with micro deep hole array" MICROMECHATRONICS AND HUMAN SCIENCE, 1998. MHS '98. PROCEEDINGS OF THE 1998 INTERNATIONAL SYMPOSIUM ON NAGOYA, JAPAN 25-28 NOV. 1998, PISCATAWAY, NJ, USA, IEEE, US, 25 November 1998 (1998-11-25), pages 177-182, XP010321839 ISBN: 0-7803-5130-4 the whole document	1-3
	-/-	

INTERNATIONAL SEARCH REPORT

International Application No
..../IB2004/050709

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	FUCHS H V ET AL: "Einsatz mikro-perforierter Platten als Schallabsorber mit inhärenter Dämpfung" ACUSTICA, S: HIRZEL VERLAG, STUTTGART, DE, vol. 81, 1995, pages 107-116, XP002097650 ISSN: 0001-7884 the whole document -----	1-3

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/IB2004/050709

Patent document cited in search report		Publication date		Patent family member(s)	Publication date
US 6414489	B1	02-07-2002	NONE		
US 2003016018	A1	23-01-2003	DE	10134540 C1	06-03-2003
DE 19838390	A	02-03-2000	DE	19838390 A1	02-03-2000
US 5084676	A	28-01-1992	JP	1915874 C	23-03-1995
			JP	3032643 A	13-02-1991
			JP	6014913 B	02-03-1994
			JP	2168936 A	29-06-1990
			JP	2886871 B2	26-04-1999
EP 0350640	A	17-01-1990	DE	68927749 D1	20-03-1997
			DE	68927749 T2	12-06-1997
			EP	0350640 A2	17-01-1990
			JP	1852235 C	21-06-1994
			JP	2084935 A	26-03-1990
			JP	5068973 B	30-09-1993
			US	4954781 A	04-09-1990
JP 2002085368	A	26-03-2002	NONE		
EP 0522742	A	13-01-1993	JP	2982392 B2	22-11-1999
			JP	5015508 A	26-01-1993
			DE	69215985 D1	30-01-1997
			DE	69215985 T2	12-06-1997
			EP	0522742 A1	13-01-1993
			US	5309105 A	03-05-1994
JP 62239503	A	20-10-1987	JP	1775260 C	28-07-1993
			JP	4061484 B	01-10-1992
DE 3444388	A	01-08-1985	DE	3444388 A1	01-08-1985
			FR	2557351 A1	28-06-1985
			JP	61082152 A	25-04-1986
			NL	8403654 A	01-07-1985
US 4774486	A	27-09-1988	JP	61278741 A	09-12-1986
			JP	1703858 C	14-10-1992
			JP	3070490 B	07-11-1991
			JP	61279238 A	10-12-1986
			DE	3677344 D1	07-03-1991
			EP	0225390 A1	16-06-1987
			WO	8607459 A1	18-12-1986
US 5256969	A	26-10-1993	JP	3173530 A	26-07-1991

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